Tomography and Radon transform

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28 March 2025

Mathematical tomography is a section of mathematics that describes methods for determining the structure of an object using scattering data. Such problems arise in microscopy, medicine, and technical control. In this report, we will write out the basic differential equation of X-ray tomography. In the course of its solution, the Radon transform arises. We will establish a connection between the Fourier transform and the Radon transform, and get acquainted with the methods of its inversion.

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- 2a. electron tomography uses electrons as a probing instrument;
- 2b. neutron tomography uses neutrons,
- 2c. neutrino tomography uses neutrinos,
- 3. acoustic tomography uses sound and ultrasound waves as a probing instrument.

Tomographies that use waves as a probing tool are called *inverse scattering problems*. The following types of tomography arise in many applications:

- medical applications (fluorography, radiography of various organs),
- technical control (baggage control at airports, monitoring the distribution of isotopes at nuclear power plants),

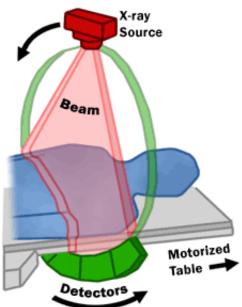
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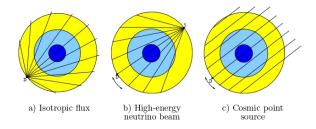
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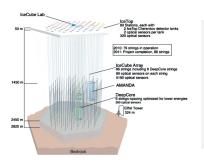
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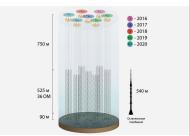






 ${\bf Fig.~1}~$ Three different approaches to "Whole Earth Tomography" using neutrino absorption. The lines refer to different baselines.

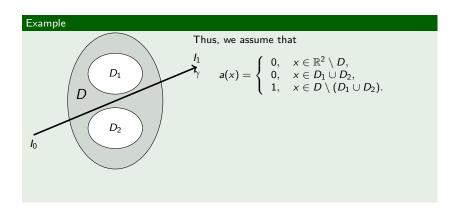


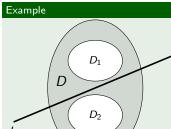


The word tomography comes from the Greek words $\tau o\mu o\varsigma$ - section, cross-section, layer, and $\gamma \rho \alpha \phi o$ - image, drawing. In tomography, the reconstruction of the structure of an object occurs, as a rule, layer by layer. At the mathematical level, in X-ray tomography, we are talking about the reconstruction of the coefficient a(x), $x \in \mathbb{R}^3$, the absorption of the radiation of X-ray photons.

Example

Let us consider a model of a section of the human body at the level of the lungs. Let $D\subseteq R^2$ be a convex compact (section of the body), $D_1\subseteq D$, $D_2\subseteq D$ be convex non-intersecting compacts (sections of the lungs). The absorption coefficient in the lungs and in water is slightly higher than zero and can be approximately considered equal to zero. In the part of the section of the body that does not contain the lungs, the attenuation coefficient of X-ray photons can be considered approximately equal to unity, which corresponds to the approximate value of the absorption coefficient in water



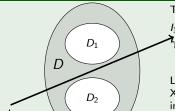


Thus, we assume that

$$a(x) = \left\{ \begin{array}{ll} 0, & x \in \mathbb{R}^2 \setminus D, \\ 0, & x \in D_1 \cup D_2, \\ 1, & x \in D \setminus (D_1 \cup D_2). \end{array} \right.$$

Let γ be an arbitrary oriented line along which X-ray photons propagate. Let I_0 be the radiation intensity before passing through the body (initial intensity), and let I_1 be the radiation intensity after the photon beam passes through the body.

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We know the value of $\frac{I_1}{I_0}$ for a sufficiently large set of oriented lines γ . We need to reconstruct the absorption coefficient of X-ray photons a(x).



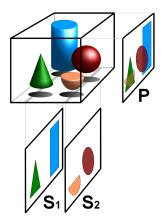
One of the main formulas of X-ray tomography, which allows to formulate the mathematical problem of restoring a(x), is based on the Beer–Bouguer–Lambert law and looks like this:

$$I_1(\gamma) = I_0 \exp\left(-\int_{\gamma} a(x) dx\right).$$
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The mathematical foundations of X-ray tomography were given in the works of [Radon, 1917], [John, 1937], [Cormack, 1963], Gelfand and co-authors (in the 1960s and later), [Helgason, 1965]. In 1979, mathematician Alan Cormack and engineer Godfrey Hounsfield received the Nobel Prize in Physiology or Medicine for the synthesis of ideas that led to the creation of the first X-ray tomograph.



Beer-Bouguer-Lambert law:

$$I_1(\gamma) = I_0 \exp\left(-\int_{\gamma} a(x) dx\right)$$

source: wiki.

Differential equation

$$\theta \nabla_{\mathbf{x}} \psi + \mathbf{a}(\mathbf{x}) \psi = 0, \ \psi = \psi(\mathbf{x}, \theta), \ \mathbf{x} \in \mathbb{R}^3, \ \theta \in S^{d-1}, \tag{2}$$

is called the *basic differential equation of X-ray tomography*. The parameter θ is called the *spectral parameter*.



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is called the *basic differential equation of X-ray tomography*. The parameter θ is called the *spectral parameter*. We assume that the function a(x) is sufficiently regular and localized (rapidly decreasing at infinity). Now, we also assume that the function a(x) is known.

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The absorption coefficient of X-ray photons a(x) is defined by the formula

$$-a(x)\psi(x,\theta) := \lim_{\varepsilon \to 0} \frac{\psi(x+\varepsilon\theta,\theta) - \psi(x,\theta)}{\varepsilon}.$$
 (4)

On the right side the derivative in the direction θ of the function $\psi(x)$ is given. Assume the function $\psi(x,\theta)$ to be sufficiently smooth. We can rewrite this definition of the absorption coefficient as an equation (2).



Let us consider a special solution $\psi^+(x,\theta)$ of the equation (2), characterized by the limit condition

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$$S(x,\theta) := \lim_{s \to +\infty} \psi^{+}(x + s\theta, \theta), \quad x \in \mathbb{R}^{d}, \quad \theta \in S^{d-1},$$
 (6)

called spectral data (or scattering data).



Note that:

$$S(x + \tau \theta, \theta) = S(x, \theta), \ S(x, \theta) = S(\pi_{\theta}x, \theta),$$

where π_{θ} is the orthogonal projection onto the plane $X_{\theta} = \{x \in \mathbb{R}^d \mid x\theta = 0\}.$

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We interpret the points $\gamma = (x, \theta) \in TS^{d-1}$ as oriented lines

$$\gamma = (x, \theta) = \left\{ y \in \mathbb{R}^d \mid y = x + s\theta, \ s \in \mathbb{R} \right\}, \text{ vector } \theta \text{ defines orientation.}$$

Thus, we interpret TS^{d-1} as the set of all oriented lines in \mathbb{R}^d .



The direct problem for the differential equation (2): given absorption coefficient a(x), find the functions $\psi^+(x,\theta)$, and then the spectral data $S(x,\theta)$:

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The inverse problem for the differential equation (2) consists of finding the absorption coefficient a(x) from the given spectral data $S(x, \theta)$:

$$S \mapsto a$$
.

The solution to the direct problem is given by the following formulas. The function ψ^+ is given by the formula

$$\psi^{+}(x,\theta) = \exp(-Da(x,-\theta)), \tag{8}$$

where $Da(x,\theta):=\int_0^{+\infty}a(x+s\theta)\,ds$ is divergent beam transform.



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$$S(x,\theta) = \exp(-Pa(x,\theta)), \ Pa(x,\theta) := \int_{\mathbb{R}} a(x+s\theta) \, ds = \int_{y \in \gamma = (x,\theta)} a \, dy. \tag{9}$$

The transformation P is called the $Radon\ transform\ along\ lines\ or\ the\ X-ray\ transform.$



The formula for the spectral data S follows from the definition (6) and from the formula (8) for the function ψ^+ . To obtain the formula (8), we are looking for the solution ψ^+ of the equation (2) in the form $\psi^+(x,\theta)=\exp(\varphi^+(x,\theta))$. Then for the function φ^+ we get the problem

$$\theta \nabla_{\mathbf{x}} \varphi^+ + \mathbf{a}(\mathbf{x}) = 0, \quad \lim_{s \to -\infty} \varphi^+(\mathbf{x} + s\theta, \theta) = 0.$$

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The X-ray transform and the Fourier transform

X-ray transform of a function f(x), $x \in \mathbb{R}^d$, as defined

$$Pf(x,\theta) = \int\limits_{\mathbb{R}^d} f(x+s\theta) ds, \quad (x,\theta) \in TS^{d-1}.$$
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$$\hat{f}(\xi) = (2\pi)^{-\frac{d}{2}} \int_{\mathbb{R}^d} e^{i\xi x} f(x) dx, \quad \xi \in \mathbb{R}^d,$$

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we also define the Fourier transform of the X-ray transform $P_{ heta}f$ by the formula

$$(P_{\theta}f)^{\wedge}(\xi) = (2\pi)^{-\frac{d-1}{2}} \int_{X_{\theta}} e^{i\xi x} P_{\theta}f(x) dx, \quad \xi \in X_{\theta}, \ \theta \in S^{d-1}.$$



[Projection theorem] We have that

$$(2\pi)^{\frac{1}{2}}\hat{f}(\xi) = (P_{\theta}f)^{\wedge}(\xi), \quad \xi \in X_{\theta}, \ \theta \in S^{d-1}.$$
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Proof.

The proof follows from the following equalities:

$$\int\limits_{X_{\theta}}e^{i\xi x}P_{\theta}f(x)dx=\int\limits_{X_{\theta}}e^{i\xi x}\int\limits_{\mathbb{R}}f(x+s\theta)\,ds\,dx=[\xi\theta=0]=\int\limits_{\mathbb{R}^{d}}e^{i\xi y}f(y)\,dy.$$



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The projection theorem allows us to reconstruct the function f from the X-ray transform Pf using the scheme

$$Pf \mapsto \hat{f} \mapsto f$$
.



Note also that in order to recover the value of the function f at the point $x \in \mathbb{R}^d$, we only need to be able to restore the values of a function defined in \mathbb{R}^2 . Actually, in order to recover the value of the function f at the point $x \in \mathbb{R}^d$, we only need to draw a two-dimensional plane $\Xi \simeq \mathbb{R}^2$ through the point x and to apply the reconstruction scheme to the function $f|_{\Xi}$. Thus, we find the value of the function f at the point f. Therefore, below we will consider the case f and the point f at the point f

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There is an isomorphism $TS^1\simeq \mathbb{R}\times S^1$, the isomorphism is given by the formulas

$$\begin{split} (s,\theta) \in \mathbb{R} \times S^1 &\mapsto (s\theta^{\perp},\theta) \in TS^1, \\ (x,\theta) \in TS^1 &\mapsto (x\theta^{\perp},\theta) \in \mathbb{R} \times S^1, \end{split}$$

where $\theta=(\theta_1,\theta_2)\in S^1$, $\theta^\perp=(-\theta_2,\theta_1)$ — the vector obtained by rotating the vector θ by a right angle counterclockwise.

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where $\theta=(\theta_1,\theta_2)\in S^1$, $\theta^\perp=(-\theta_2,\theta_1)$ — the vector obtained by rotating the vector θ by a right angle counterclockwise. Therefore, for the case d=2

$$\hat{f}(r\theta^{\perp}) = (2\pi)^{-1} \int_{\mathbb{R}} e^{irs} q_{\theta}(s) ds, \qquad (12)$$

where $q_{\theta}(s) := Pf(s\theta^{\perp}, \theta)$, $s \in \mathbb{R}$, $\theta \in S^1$.



Radon formula

Theorem (Radon, 1917)

The following formula holds:

$$\begin{split} f(x) &= \frac{1}{4\pi} \int\limits_{\mathcal{S}^1} \theta^\perp \nabla \tilde{q}_\theta(x \theta^\perp) \, d\theta, \quad x \in \mathbb{R}^2, \\ \tilde{q}_\theta(s) &= (Hq_\theta)(s) := \frac{1}{\pi} \text{p.v.} \int\limits_{\mathbb{R}} \frac{q_\theta(t)}{s - t} \, dt, \\ q_\theta(s) &= Pf(s \theta^\perp, \theta), \quad s \in \mathbb{R}, \; \theta = (\theta_1, \theta_2) \in \mathcal{S}^1, \; \theta^\perp = (-\theta_2, \theta_1). \end{split}$$

The function $\tilde{q}_{\theta}(s)$ is called the filtered backprojection.



Radon formula

Here p.v. denotes the integral in the sense of the principal value:

$$\text{p.v.} \int_{\mathbb{R}} \frac{u(t)}{s-t} dt := \lim_{\varepsilon \to +0} \left[\int_{-\infty}^{s-\varepsilon} + \int_{s+\varepsilon}^{+\infty} \right] \left(\frac{u(t) dt}{s-t} \right)$$
$$\equiv \lim_{\varepsilon \to +0} \int_{\mathbb{R}} \frac{1}{2} \left(\frac{1}{s-t+i\varepsilon} + \frac{1}{s-t-i\varepsilon} \right) u(t) dt.$$

For the numerical calculation of integrals in the sense of the principal value, the following formula based on the residue theorem can be used:

$$\int\limits_{\mathbb{R}} e^{-ips} ds \, \mathrm{p.v.} \int\limits_{\mathbb{R}} \frac{u(t)}{s-t} \, dt = -i\pi p \int\limits_{\mathbb{R}} e^{-ipt} u(t) \, dt.$$

Radon's formula is now the basic one in applications. It is a basis for *filtered backprojection algorithm*).



Radon formula

Proof.

Using the expression for the inverse Fourier transform in polar coordinates, we obtain:

$$f(x) = (2\pi)^{-1} \int_{S^{\perp}} \int_{0}^{+\infty} e^{-ir\theta^{\perp}x} \hat{f}(r\theta^{\perp}) r \, dr \, d\theta$$

$$= \frac{1}{4\pi} \int_{S^{\perp}} \int_{\mathbb{R}} e^{-ir\theta^{\perp}x} \hat{f}(r\theta^{\perp}) r sgnr \, dr \, d\theta = \frac{1}{8\pi^{2}} \int_{S^{\perp}} \int_{\mathbb{R}} \int_{\mathbb{R}} e^{ir(s-\theta^{\perp}x)} q_{\theta}(s) \, ds \, r sgnr \, dr \, d\theta.$$

Next, since

$$\int\limits_{\mathbb{R}}e^{irs}(-i)sgnr\,dr=\frac{1}{s+i0}+\frac{1}{s-i0} \text{ (in the sense of distributions)},$$

we obtain the theorem



Theorem (Cormack (1963–1964), d = 2; Helgason (1965), $d \ge 2$)

Let $f \in \mathcal{S}(\mathbb{R}^d)$. $R_{2,1}f|_{\Omega_{d,d-1}(B_r)}$ defines $f|_{\mathbb{R}^d \setminus B_r}$.

Using polar coordinates, we represent the coordinates x_1 and x_2 as $x_1 = r\cos\varphi$, $x_2 = r\sin\varphi$ and expand the function f(x) in a Fourier series in the variable φ for each fixed r:

$$f(x) = \sum_{l=-\infty}^{+\infty} f_l(r) e^{il\varphi}.$$
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Let $\theta=(\cos\varphi,\sin\varphi)$, $\theta^{\perp}=(-\sin\varphi,\cos\varphi)$. We expand the X-ray transform in a Fourier series in the variable $\left(\varphi+\frac{\pi}{2}\right)$ for each fixed s $P(s\theta^{\perp},\theta)$:

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$$P(s\theta^{\perp},\theta) = \sum_{l=-\infty}^{+\infty} q_l(s)e^{il\left(\varphi + \frac{\pi}{2}\right)}.$$
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It is sufficient to show that $f_l(r)$ for $r \ge \rho$ depends only on $q_l(s)$ $s \ge \rho$.



Theorem (Cormack Formulas (1963–1964))

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$$q_{l}(s) = 2 \int_{s}^{+\infty} T_{|l|} \left(\frac{s}{r}\right) \left(1 - \frac{s^{2}}{r^{2}}\right)^{-\frac{1}{2}} f_{l}(r) dr, \quad s > 0,$$
 (15)

$$f_{l}(r) = -\frac{1}{\pi} \int_{r}^{+\infty} (s^{2} - r^{2})^{-\frac{1}{2}} T_{|l|} \left(\frac{s}{r}\right) q'_{l}(s) ds, r > 0.$$
 (16)



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$$f_l(r) = -\frac{1}{\pi} \int_{r}^{+\infty} (s^2 - r^2)^{-\frac{1}{2}} T_{|I|} \left(\frac{s}{r}\right) q_l'(s) ds, r > 0.$$
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$$T_0(x) \equiv 1$$
, $T_1(x) = x$, $T_{l+1}(x) + T_{l-1}(x) = 2xT_l(x)$, $l = 1, 2, ...$,

2 by an explicit formula:

$$T_I(x) = \left\{ egin{array}{ll} \cos(I\arccos x), & |x| \leqslant 1, \ \cosh(Ix), & |x| \geqslant 1, \end{array}
ight. x \in \mathbb{R}.$$



Thanks for your attention!